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Repetition Suppression Dissociates Spatial Frames of Reference  
in Human Saccade Generation

Running title: Repetition suppression during saccade generation

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37 **Abstract**

38 The path from perception to action involves the transfer of information across  
39 various reference frames. Here we applied an fMRI repetition suppression (RS)  
40 paradigm to determine the reference frame(s) in which the cortical activity is  
41 coded at several phases of the sensorimotor transformation for a saccade,  
42 including sensory processing, saccade planning and saccade execution. We  
43 distinguished between retinal (eye-centered) and non-retinal (e.g., head-  
44 centered) coding frames in three key regions: the intraparietal sulcus (IPS),  
45 frontal eye field (FEF) and supplementary eye field (SEF). Subjects (n=18)  
46 made delayed-saccades to one of five possible peripheral targets, separated at  
47 intervals of 9° visual angle. Target locations were chosen pseudo-randomly,  
48 based on a 2x2 factorial design with factors retinal and non-retinal coordinates  
49 and levels novel and repeated. In all three regions, analysis of the BOLD  
50 dynamics revealed an attenuation of the fMRI signal in trials repeating the  
51 location of the target in retinal coordinates. The amount of retinal suppression  
52 varied across the three phases of the trial, with the strongest suppression  
53 during saccade planning. The paradigm revealed only weak traces of non-  
54 retinal coding in these regions. Further analyses showed an orderly  
55 representation of the retinal target location, as expressed by a contralateral bias  
56 of activation, in the IPS and FEF, but not in the SEF. These results provide  
57 evidence that the sensorimotor processing in these centers reflects saccade  
58 generation in eye-centered coordinates, irrespective of their topographic  
59 organization.

60

61 Keywords: saccade generation, fMRI, reference frames, repetition suppression

62

63 **Introduction**

64 To understand how the brain processes and transforms spatial information for  
65 movements, the notion of a reference frame is indispensable (Soechting and  
66 Flanders 1992). Using this concept, electrophysiological evidence from the  
67 monkey has shown that movement-related neurons employ a variety of  
68 reference frames, anchored to eyes, head, other body-parts, or world (Colby  
69 1998; Andersen and Buneo 2002; Martinez-Trujillo et al. 2004; Olson 2003).  
70 However, it is unclear to what extent this information, which is extracted from  
71 post-synaptic action potentials of a relatively small number of pyramidal  
72 neurons, can be related to the computations of larger neuronal populations  
73 (Logothetis 2008) and to other species, including humans.

74 Data on spatial reference frames of large neuronal assemblies in the  
75 human brain are still scarce. A few recent fMRI studies addressed this issue  
76 using topographic mapping procedures. Examining how topographic maps of  
77 target locations change as a function of eye position allows to distinguish  
78 between retinal (eye-centered) or non-retinal (head/body/space centered)  
79 reference frames (Medendorp et al. 2003; Merriam et al. 2003; Sereno and  
80 Huang 2006; Gardner et al. 2008). As a result, Medendorp et al. (2003)  
81 demonstrated the existence of a retinocentric saccade-and-reach area in  
82 parietal cortex, which was recently shown to code movement goals, not motor  
83 commands (Fernandez-Ruiz et al. 2007)

84 However, neurons may not always be topographically arranged along the  
85 dimensions of the reference frame they employ. A brain area could encode  
86 information in a particular reference frame even if the respective neurons do not  
87 show an orderly spatial organization according to the value of that particular

88 parameter. This is likely the case for regions involved in movement control,  
89 where multidimensional motor constraints must be organized into a two-  
90 dimensional map (Graziano and Aflalo 2007).

91         Repetition suppression (RS) offers a potential solution to investigate the  
92 reference frames used in the neural control of movement without relying on the  
93 special case of an orderly topographic arrangement of the relevant neurons. RS  
94 is based on the observation that repeated processing of a given stimulus  
95 feature leads to a reduction of neural activity in neurons tuned to that particular  
96 feature (Desimone 1996). By varying the property of the stimulus across  
97 different dimensions, the features processed in a given brain region can be  
98 uncovered. While many fMRI studies have successfully used this technique in  
99 studies of perceptual representation (McKyton et al. 2007; see Grill-Spector et  
100 al. 2006, for review), expectation (Summerfield et al. 2008) and action  
101 observation (Hamilton and Grafton 2006, 2008; Dinstein et al. 2008; Majdandžić  
102 et al. 2009), to date this method has not been applied to examine neural  
103 representations underlying sensorimotor control.

104         In this study, we used RS methods to investigate the reference frames  
105 used to encode targets for saccadic movements in the main cortical centers for  
106 saccades in the human brain: intraparietal sulcus (IPS), frontal eye field (FEF),  
107 and supplementary eye fields (SEF). Participants executed memory-guided  
108 saccades to peripherally presented target (Figure 1A). By varying the fixation  
109 position for the next trial, we could then make the next target either identical in  
110 retinal coordinates, or in non-retinal coordinates. We found a clear reduction of  
111 the BOLD signal in all three regions on the second compared to the first trial  
112 when the target location was repeated in retinal coordinates, but not, or much

113 less, during a repetition in a non-retinal frame. Retinal suppression was stronger  
114 during saccade planning than execution. This suggests that the neural  
115 commands from these centers, of which only some have a measurable  
116 topographic distribution of spatially-tuned neurons (IPS and FEF), encode  
117 saccade goals in retinocentric coordinates.

118

## 119 **Materials and Methods**

120

### 121 *Subjects and ethical approval*

122 Eighteen healthy subjects with normal or corrected-to-normal vision participated  
123 in the study (8 female, 10 male, aged 20-37 years). Three subjects were left-  
124 handed; one subject was aware of the exact purpose of the experiment. All  
125 gave written informed consent in accordance with the guidelines of the local  
126 ethics committee (CMO Committee on Research involving Human Subjects,  
127 region Arnhem-Nijmegen, The Netherlands). Subjects practiced the task 1-2  
128 days in advance in a mock setup outside the scanner to ensure that the task  
129 and paradigm were correctly understood. In addition, a few practice trials were  
130 performed inside the scanner just prior to the experiment.

131

### 132 *Experimental setup*

133 Subjects were lying supine in the scanner, with their heads tilted 30° with  
134 respect to the scanner bed by means of a wooden support board that was  
135 attached to the bed. This enabled the subjects to view all stimuli directly without  
136 mirrors, making the task as natural as possible. Their head was fitted inside a  
137 phased-array receiver head coil. The head and neck were stabilized within the

138 head coil using foam blocks and wedges. A foam block was also placed  
139 underneath the knees, and in some subjects the elbows and neck were further  
140 supported by cushions to make them feel more comfortable.

141 A stimulus device consisting of seven horizontally placed yellow-colored  
142 light-emitting diodes (LEDs), was attached to an arch of about 40 cm height that  
143 was placed over the subject's hip, at a viewing distance of 34 cm. The central  
144 LED was aligned with the subject's body midline; three peripheral LEDs were  
145 located on either side, at an eccentricity of 4.5, 9 and 18° from the central LED.  
146 This configuration allowed subjects to view all stimuli with a comfortable, slightly  
147 downward gaze direction relative to the head.

148 Stimulus LEDs were controlled using Presentation software  
149 (Neurobehavioral Systems, San Francisco, CA, USA). Position of the left eye  
150 was recorded using a long-range infrared video-based eyetracker (SMI, Teltow,  
151 Germany) at a frequency of 50 Hz.

152

### 153 *MR settings*

154 Anatomical and functional images were obtained on a Siemens 3 Tesla MRI  
155 scanner (Siemens Trio, Erlangen, Germany). Functional images consisted of 32  
156 axial slices acquired by a gradient-echo planar imaging sequence using an  
157 eight-channel phased-array receiver head coil (slice thickness 3.0 mm, gap =  
158 17%, in-plane pixel size 3.5 x 3.5 mm, TR = 2000 ms, TE = 35 ms, FOV = 224  
159 mm, flip angle = 80°). In total, 1140 functional images were obtained in one run,  
160 lasting 35 minutes. Hereafter, high-resolution anatomical images were acquired  
161 using a T1-weighted MP-RAGE sequence (192 sagittal slices, voxel size 1.0 x  
162 1.0 x 1.0 mm, TR = 2300 ms, TE = 2.02 ms, FOC = 256 mm, flip angle = 8°).

163

164 *Experimental paradigm*

165 The experiment took place in complete darkness; only the stimulus LEDs were  
166 visible. Subjects performed a memory-guided saccade task, using a rapid  
167 event-related repetition suppression (RS) design (Figure 1A, upper panel). A  
168 trial started with a subject fixating an illuminated stimulus LED (Fixation Point,  
169 F). Then, after a period of 3 s, one of the other stimulus LEDs flashed for 200  
170 ms, which served as the target stimulus (S) for the pending saccade. This was  
171 followed by a 3.8 s memory delay during which the subject maintained fixation  
172 on F. Subsequently, F was extinguished, which was the go-cue for the subject  
173 to make the saccade to S, as accurately as possible. Then, 1 s later, the next  
174 trial started, with an intermediate refixation saccade to change F to a different  
175 location than S in the previous trial. Each trial lasted eight seconds. Trial lengths  
176 were not jittered to rule out potential confounding effects caused by the  
177 nonlinear nature of RS (Van Turennout and Martin 2003). Furthermore, the trial  
178 sequence was chosen such that correlation between the fMRI-regressors  
179 describing the BOLD-signal during the delay period was low (<0.3). The total  
180 experiment consisted of 36 blocks of 4 trials, yielding a total of 144 trials.

181 In each trial, both F and S could be presented at one of five possible  
182 locations, at  $-18^\circ$ ,  $-9^\circ$ ,  $0^\circ$ ,  $+9^\circ$  or  $+18^\circ$  from the center. Combinations of F and S  
183 were chosen pseudo-randomly; we did not test trials in which  $S=F$  since this  
184 implied no saccadic response. In the majority of trials (85 %), the angular  
185 separation between F and S was  $9^\circ$  to exploit the fact that  $9^\circ$  saccades may  
186 drive higher BOLD responses than larger amplitude saccades, based on the

187 overrepresentation of the central visual field in several visual and oculomotor  
188 regions (Ben Hamed et al. 2001).

189         Because the head and body were fixed during the experiment, head,  
190 body, and space-centered reference frames can be treated as equivalent, and  
191 are therefore referred to as a non-retinal reference frame. Likewise, under the  
192 present conditions, retinocentric, eye-centered and gaze-centered reference  
193 frames can be considered synonymous notions, and referred to as a retinal  
194 reference frame.

195         Repetition suppression effects were elicited by systematically  
196 manipulating target location over successive trials in a 2x2 design, with  
197 conditions retinal and non-retinal coordinates (labeled as R and N,  
198 respectively), and levels novel and repeated (labeled as n and r, respectively).  
199 E.g., as illustrated in Figure 1A, the retinal location of a target presented in trial  
200 t, could be repeated in the next trial t+1, while the non-retinal location was novel  
201 (lower left panel; retinal repeated, non-retinal novel; RrNn). Alternatively, the  
202 retinal location of the target in trial t+1 could be novel compared to the  
203 preceding trial t, while the non-retinal location was repeated (RnNr, lower right  
204 panel). Finally there were two types of trials (not shown) in which the location of  
205 the target was either repeated or novel in both coordinate frames (RrNr and  
206 RnNn, respectively).

207         The first trial of each block was not included in the RS analysis in order to  
208 avoid carry-over effects from the previous block (we used these trials to define  
209 our oculomotor regions-of-interest, see below). The remaining 108 trials  
210 consisted of 36 RnNn trials, and 24 trials of each of the other three types of  
211 trials (RrNn, RnNr, RrNr). A target's retinal or non-retinal location was never

212 repeated more than once in a row in order to get the strongest RS effects and  
213 avoid adaptation fatigue (Van Turenout et al. 2003). Target directions were  
214 balanced across the visual and craniotopic hemifields; average amplitudes were  
215 the same across the four conditions. The intermediate saccades between trials  
216 to change initial fixation points were also chosen such that on average they  
217 could not explain any RS effect in either reference frame.

218         After each block of four trials, subjects performed a so-called washout  
219 task to allow the BOLD signal to return to baseline level after several RS trials,  
220 alleviating possible longer lasting RS effects (Majdandžić et al. 2009). The start  
221 of this washout task was indicated by three brief subsequent flashes of two  
222 targets (first  $-4.5^{\circ}/+4.5^{\circ}$ , then  $-9^{\circ}/+9^{\circ}$ , finally  $-18^{\circ}/18^{\circ}$ ), followed by the onset of  
223 the central LED for a jittered duration (1.4-12.6 s). Subjects were instructed to  
224 fixate this LED and track it as it subsequently jumped to different locations after  
225 each 250 ms, eight times in total. These locations were balanced across  
226 directions and were evenly distributed across the 7 LEDs on the stimulus  
227 device. The washout task ended by a period of central fixation (1.4-14.0 s)  
228 followed by again the same three short flashes, but now in opposite order. Each  
229 washout period lasted 15.2 – 32.0 s (mean 23.1 s). After each 6 blocks and  
230 their associated washouts, subjects had a rest period of 30 s, during which  
231 there was no visual stimulation and they could freely move their eyes. The total  
232 experiment lasted 60 minutes, including practice and anatomical scanning.

233

#### 234 *Behavioral analysis*

235 Eye movement data (horizontal component) were processed separately per  
236 block of four trials and calibrated in degrees based on the fixation data of the

237 following washout period. This generally yielded calibration accuracies better  
238 than  $1.5^\circ$ . Figure 1B show the eye traces of a typical subject from central  
239 fixation to a remembered target location at either  $9^\circ$  (gray) or  $-9^\circ$  (black), in  
240 relation to the temporal order of events (see Fig 1A). As shown, this subject  
241 maintained fixation during the presentation of the target cue, and made eye  
242 movements with latencies of about 200 ms in the correct directions after the  
243 fixation target was turned off. Due to technical problems, eye-movement data of  
244 one subject were lost for the last 12 blocks of trials. We used the eye recordings  
245 to identify error trials, which were defined as trials in which subjects did not  
246 keep fixation when required, or made saccadic responses that were anticipatory  
247 or into the wrong direction. Although the temporal resolution (20 ms) was  
248 relatively course, eye traces were also used to determine reaction times. On  
249 average,  $9 \pm 4$  (SD) trials per subject were discarded based on these criteria.  
250 For the remaining trials, average fixation accuracy was  $1.8^\circ$  (SD =  $1.4^\circ$ ) across  
251 subjects. Accuracy of saccades to the remembered targets, in degrees of visual  
252 angle, was  $3.0^\circ$  (SD =  $1.2^\circ$ ) across conditions. This confirmed that the saccades  
253 were driven by the memory of the actual targets and were not simply guided  
254 stereotypically to the left or right.

255

#### 256 *Preprocessing of fMRI data*

257 fMRI data were analyzed using BrainVoyager QX (Brain Innovation, Maastricht,  
258 The Netherlands). Subsequent analyses were performed using Matlab (The  
259 Mathworks). The first five volumes of each subject's data set were discarded to  
260 allow for T1 equilibration. Functional data were first corrected for slice scan time  
261 acquisition and motion. Subsequently, the data were temporally filtered using a

262 high-pass filter with a cutoff frequency of 1/268 s. The functional images were  
263 co-registered with the anatomical scan and transformed into Talairach  
264 coordinate space using the nine-parameter landmark method (Talairach and  
265 Tournoux 1988). Finally, the images were smoothed with an isotropic Gaussian  
266 kernel of 8-mm full-width-at-half-maximum.

267

### 268 *Statistical inference and regions of interest*

269 The goal of the study is to use repetition suppression to investigate the  
270 reference frames employed in the three key cortical centers for saccades; the  
271 IPS, FEF and SEF. We used the first trials (referred to below as localizer trials)  
272 of each block to identify these regions, while the other trials (below referred to  
273 as RS trials) in the block subserved the RS analysis in the regions. This split of  
274 the data was done to avoid any circular analyses of the data (see Kriegeskorte  
275 et al. 2009).

276 For each subject we defined 19 regressors. Four of these were used in  
277 relation to localizing the ROIs. More specifically, one regressor specified the 2-s  
278 fixation period of the localizer trials as well as the fixation periods in the washout  
279 task, the second, third and fourth regressors specified the stimulus period, the  
280 memory interval and the saccade periods of the localizer trials.

281 Seven regressors were modeled in relation to studying the RS effects,  
282 based on using the RS trials. The first modeled the 2-s fixation periods at the  
283 beginning of each trial. The second regressor captured the periods of 0.2 s  
284 during which the target stimulus was presented. Four other regressor functions  
285 characterized the subsequent working memory interval according to the 2 x 2  
286 design of conditions Retinal (R) and Non-retinal (N) locations with levels Novel

287 (n) and Repeated (r). These regressors (RnNn, RrNn, RnNr, and RrNr) covered  
288 the 3.8 s delay period starting with target offset until fixation point offset (go  
289 cue). Saccade periods of the RS trials were modeled by the seventh regressor,  
290 which included the first second after the go cue and the first second after  
291 presentation of the fixation LED of the next RS trial.

292 In addition to these eleven regressors, we used eight regressors of non-  
293 interest. One modeled the delay periods of error trials; another characterized  
294 the periods of rest and the intervals in which the cues for the start and end of  
295 the washout period were presented. All regressors were defined as boxcar-  
296 functions over the time interval they described and were convolved with a  
297 hemodynamic response function (modeled using a two-gamma model function  
298 with response undershoot ratio of 6, time to response peak of 5 s and time to  
299 undershoot peak of 15 s). The final six regressor functions represented the  
300 head motion, based on the six parameters provided by BrainVoyager's motion-  
301 correction algorithm.

302 Individual subject GLMs were corrected for serial correlations in the time  
303 courses. Random effects group analyses were performed to test effects across  
304 subjects, using the false discovery rate (FDR) controlling procedure to correct  
305 for multiple comparisons, at the  $q(\text{FDR}) < 0.01$  significance level (Genovese et al.  
306 2002). Using a random-effects group analysis, we first determined the regions  
307 that show significant activity during oculomotor preparation and execution in the  
308 localizer trials. From the activation maps, we selected three bilateral regions of  
309 interest (ROI), known to be important regions in saccade generation: FEF, SEF  
310 and a region in the intraparietal sulcus (IPS). Each ROI was defined as all the  
311 contiguous voxels that exceeded a threshold of  $q(\text{FDR}) < 0.05$  within a cubic

312 cluster of 8x8x8 mm (to match the smoothing kernel), centered at the points of  
313 peak activation.

314

### 315 *Linear deconvolution*

316 In a second analysis, we used finite impulse response deconvolution to extract  
317 the activation profiles in the ROIs for each of the four RS conditions (RnNn,  
318 RrNn, RnNr, and RrNr). In this approach, the BOLD data were first resampled  
319 into 0.5 s time intervals. Then, for each condition, a set of 31 impulse responses  
320 (one impulse per 0.5-s volume) was aligned to the start of each trial in the  
321 group. Together, the 31 impulse regressors for a given condition modeled the  
322 activation time course for trials in this condition with two points per second over  
323 15 s. Thus, each group of trials yielded 31 columns to a subject's GLM design  
324 matrix, with ones at the appropriate locations, to model the 31 impulse functions  
325 for that trial group (Dale 1999; Serences 2004; Brown et al. 2006). Fitting this  
326 design matrix to the resampled data automatically deconvolves the time series  
327 of each RS condition (Brown et al. 2006), without making any assumption about  
328 the shape of the activation profile, other than its length (15 s in this case).  
329 Because of the random ordering of the four trial types, effects of previous trials  
330 are balanced out in this analysis (is assumed that the haemodynamic response  
331 is linear), as is shown in Fig 3, where all time traces start from the same  
332 baseline. Next, for each RS condition and each ROI, a mean signal and  
333 standard deviation were computed across subjects. Differences between  
334 conditions capture the RS effects in either reference frame. That is, retinal RS  
335 follows from  $(RnNn + RnNr) - (RrNn + RrNr)$  and non-retinal RS is computed as

336 (RnNn + RrNn) – (RnNr + RrNr). Statistical significance was tested using paired  
337 t-tests and repeated-measures ANOVAs at the  $P < 0.05$  confidence level.

338

## 339 **Results**

340

### 341 *Behavioral performance*

342 Subjects performed memory guided saccades to targets whose coordinates  
343 were systematically manipulated in both retinal and non-retinal coordinates  
344 (labeled as R and N, respectively). Thus, with respect to the previous trial,  
345 target locations could be novel in both retinal and non-retinal coordinates  
346 (RnNn, see Figure 1A), repeated in both reference frames (RrNr), or novel in  
347 one, but repeated in the other frame (RnNr and RrNn).

348 Table 1 shows performance (defined as correct fixation and saccade  
349 direction) and saccade latencies for each of these four trial types. Across  
350 subjects, performance was >93% correct, in all conditions. A 2x2 repeated-  
351 measures ANOVA with repeated versus non-repeated trials and retinal versus  
352 non-retinal target locations as factors revealed no significant main  
353 ( $F(1,17) < 3.98$ ,  $P > 0.062$ ) or interaction effect ( $F(1,17) = 1.30$ ,  $P = 0.27$ ). The mean  
354 latency of the saccadic response was  $217 \pm 69$  ms (mean + SD) across the four  
355 conditions. The differences among the four conditions were not statistically  
356 significant ( $F(1,17) < 0.86$ ,  $P > 0.36$ ). Finally, there were no differences either in  
357 performance or in saccadic latency between the first and second half of the  
358 performed trials (t-test,  $P < 0.01$ ). Together, the behavioral results indicate that  
359 possible differences in corresponding fMRI activations cannot be related to  
360 different levels of task performance.

361

362 *fMRI activation data*

363

364 *Activation maps during delay period*

365 Using a random-effects group GLM analysis across all 18 subjects, we first  
366 identified the cortical areas involved in saccade generation using the localizer  
367 trials (see Methods). Figure 2A and B show two anatomical views of these  
368 results, in neurological convention, thresholded at  $q(\text{FDR}) < 0.01$ . In Fig 2C and  
369 D, this activation map is rendered onto an inflated representation of the left  
370 hemisphere of one of the subjects. Consistent with previous results, a bilateral  
371 network of eye-movement related cortical areas was activated (Schluppeck et  
372 al. 2005; Curtis and D'Esposito 2006; Brown et al. 2004; Connolly et al. 2002).  
373 This included a region along the intraparietal sulcus (IPS), which might be the  
374 human analog of monkey area LIP (Medendorp et al. 2003; Connolly et al.  
375 2007; Sereno et al. 2001). In the frontal cortex, we found significant voxels at  
376 the junction of the precentral sulcus and the superior frontal sulcus, probably  
377 corresponding to the frontal eye field (FEF; Paus et al. 1996; Brown et al. 2004).  
378 More medially, significant voxels were found along the interhemispheric fissure,  
379 extending onto the dorsal cortical surface, which can be classified as the  
380 supplementary eye field (SEF; Picard and Strick 2001; Grosbras et al. 1999;  
381 Brown et al. 2004). Finally, more laterally in the left frontal cortex, significant  
382 responses were found in voxels covering the precentral sulcus, corresponding  
383 to the ventral premotor area (PMv; Picard and Strick 2001; Beurze et al. 2007).

384 Table 2 lists the mean Talairach coordinates (in mm) of the peak voxel  
385 within each region, together with the corresponding t-values across subjects.

386 From these regions, we subjected the bilateral regions IPS, FEF, and SEF,  
387 each defined as all contiguous voxels exceeding a threshold of  $q(\text{FDR}) < 0.05$   
388 within a cubic cluster of 8x8x8 mm, to a careful investigation of the RS effects.

389

#### 390 *Reference frame-dependent repetition suppression*

391 Can repetition suppression reveal which frames of reference are used to code  
392 the representation in these oculomotor regions? Given our hypotheses, we may  
393 predict that, when the retinal location of a target is repeated in subsequent  
394 trials, voxels will show an attenuation of their BOLD-activation when the  
395 underlying neuronal populations code target location in a retinal reference  
396 frame, but not if they code in a non-retinal reference frame. Conversely, regions  
397 that code the non-retinal (e.g. craniotopic) location of a target will only show  
398 BOLD adaptation when the non-retinal location of the target is repeated. Of  
399 course, it is also possible that a region would be best characterized by a mixture  
400 of these two frames.

401 Figure 3A shows the reconstructed BOLD response of the left and right  
402 IPS over a time course of 12 s, averaged across subjects (see Methods).  
403 Repeated trials (gray) had the same target location as the previous trial (black)  
404 in retinal coordinates. Time  $t=0$  s denotes the onset of the target stimulus;  $t=4$  s  
405 the go-cue for the saccade. As shown, in both novel and repeated trials, after  
406 the brief presentation of the target stimulus ( $t=0$  s), cortical activation during the  
407 first delay period shows first a phasic response (time interval 0 to 4 s), followed  
408 by a tonic response (time 4 - 6 s). Then, at time 7 - 10 s, there is again a strong  
409 increase in cortical activation, caused by the execution of planned saccade and  
410 the subsequent saccade to fixate a new fixation point (see Methods). The

411 activity, in particular the early phasic and tonic activity is suppressed in  
412 repeated trials compared to novel trials, in both hemispheres, which would be  
413 consistent with the prediction of the retinal model. Figure 3C illustrates this  
414 more clearly, by showing the mean difference ( $\pm$  95% confidence intervals)  
415 between the activation patterns during novel and repeated trials (average  
416 repetition suppression in retinal coordinates). Across the entire trial period,  
417 BOLD activation during repeated trials is significantly lower than during novel  
418 trials (paired t-test,  $P < 0.001$ ), with the suppression effects most pronounced  
419 during the tonic delay phase.

420 To investigate whether the retinal representation in the IPS is  
421 intermingled with a non-retinal representation, we compared novel and repeated  
422 trials with the same target location in non-retinal coordinates. As shown in  
423 Figure 3B, activation patterns during novel and repeated trials are quite similar.  
424 Their difference is plotted in Fig 3D, together with the 95% confidence intervals  
425 (gray area). Across the entire time course, and in both hemispheres, the  
426 difference in activation does not significantly deviate from zero ( $P > 0.41$ ). Thus,  
427 we found no clear evidence for a non-retinal representation, in contrast to clear  
428 findings regarding the retinal representation.

429 The results of the IPS are exemplary for those in the FEF and SEF.  
430 Therefore, to analyze the findings quantitatively for each ROI, we computed in  
431 each subject the average difference between the novel and repeated signals at  
432 three phases of the trial, indicated by the vertical gray boxes in Figure 3A. The  
433 resulting value is a measure for the amount of repetition suppression (RS  
434 value). We computed these RS values (corrected for the fMRI hemodynamic  
435 lag) for the stimulus-related activity (S: 1-3.5 s), the delay period (D: 4-6.5 s),

436 and the execution phase (E: 7.5-10 s). For each ROI, the amount of RS was  
437 determined across hemispheres, in both reference frames.

438 Figure 4 plots the average results of this analysis across the entire group  
439 of subjects. As shown, brain activations are significantly suppressed when a  
440 target location is repeated in retinal coordinates (black bars), for all ROIs and  
441 trial phases (repeated measures ANOVA;  $F(1,17) > 5.5$ ,  $P < 0.05$  in all cases).  
442 Retinal suppression was strongest during the delay phase. This confirms the  
443 observations in Figure 3 and illustrates the role of these regions in saccade  
444 planning. In contrast, we found only weak, non-significant suppression effects  
445 when a target location is repeated in non-retinal coordinates (white bars) during  
446 the delay phase, and not during the stimulus or execution phases.

447 The current design was not sensitive enough to test a potential  
448 magnitude effect of increasing RS with saccade size, because the set of  
449 saccades with amplitudes larger than  $9^\circ$  was too small (15%). Such an effect  
450 could be expected on basis of the cortical magnification of the central visual  
451 field in the early cortical stages of processing. However, when we constrained  
452 our analysis to only the trials with  $9^\circ$  saccades, the retinal RS values were not  
453 significantly different compared to including all trials. This was the case for all  
454 areas and trial epochs ( $P > 0.05$ ).

455 To test how much these results hold within single subjects, we  
456 determined a reference frame index (RFI) on basis of the RS effects for each of  
457 them. This index value was computed as the difference between the amount of  
458 retinal and non-retinal RS, weighted by their cumulative effect size. The  
459 histograms in Fig 5 show the distribution of these RFIs across subjects. For all  
460 regions and trial phases, there is a clear bias in the population of subjects

461 towards retinal coding. This is reflected in the average RFI, which is in all cases  
462 significantly larger than zero ( $P < 0.01$ ), with values varying between  $0.21 \pm 0.30$   
463 (mean  $\pm$  SD) (SEF, delay period) and  $0.36 \pm 0.36$  (SEF, execution phase).

464 Together, the results presented in Figs 4 and 5 provide evidence for the  
465 existence of, at least, a dominant sustained eye-centered representation in the  
466 selected saccade regions.

467

#### 468 *Contralateral bias*

469 To what extent are the RS findings of a retinal coding of target location  
470 consistent with the topographic organization of these areas, as revealed by  
471 lateralized cortical activity? Because we varied eye position, our paradigm  
472 allows us to distinguish between lateralized activity in retinal and non-retinal  
473 coordinates. If the spatially-selective retinal neurons are topographically  
474 organized in the selected ROIs, we would expect that targets in the contralateral  
475 visual field will generate a higher BOLD response than targets presented in the  
476 ipsilateral hemifield. Alternatively, it is possible that the retinal RS effects are not  
477 embedded in a neural map with an orderly spatial organization. Because only  
478 retinal RS effects were seen, we anticipate that none of the regions will  
479 demonstrate non-retinal laterality.

480 To test the presence of lateralized activity in our data, we performed two  
481 GLM analyses, each using two regressors to describe target location (left or  
482 right in retinal or non-retinal coordinates) during the delay period (see also  
483 Methods). We compared the resulting beta-weights of these regressors in both  
484 GLMs, separately for each ROI. Figure 6A presents the differences between the  
485 activity elicited by contralateral and ipsilateral targets. For the IPS and FEF, a

486 strong contralateral bias was found, in retinal coordinates, which was significant  
487 across hemifields (repeated measures ANOVA;  $F(1,17) > 28.4$ ,  $P < 0.001$  in both  
488 regions). In the SEF, however, there was no significant lateralized activity  
489 ( $F(1,17) = 0.08$ ,  $P = 0.78$ ). In combination with our RS results, this suggests that,  
490 although retinal RS effects are present in the SEF, there is no contralateral bias  
491 of these spatially selective neurons in this area.

492 For completeness, when targets were sorted according to their non-  
493 retinal (head-centric) location, there was no significant difference between  
494 contralateral and ipsilateral activity in any of the regions (Figure 6B; repeated  
495 measures ANOVA;  $F(1,17) < 1.6$ ;  $P > 0.22$  in all regions). This compares well to  
496 the RS results, which do not favor the non-retinal reference frame either.

497 All together, our results show that repetition suppression can be used as  
498 a tool to distinguish between reference frames in frontoparietal areas involved in  
499 spatial memory processing for saccades, even when those regions lack a clear  
500 topographic organization.

501

## 502 **Discussion**

503 Identifying the computational architecture of the human brain has been a major  
504 aim in neuroscience research over the last decades. One of the key questions  
505 concerns the internal organization of the various brain regions involved in  
506 sensorimotor processing, i.e., how and why different regions provide different  
507 solutions to the underdetermined problem of mapping multidimensional motor  
508 constraints into a two-dimensional neuronal matrix (Graziano and Aflalo 2007;  
509 Kohonen 2001).

510 Using repetition suppression (RS) effects, we addressed a particular  
511 instance of this general issue by studying the spatial reference frames  
512 employed by three human oculomotor areas (IPS, FEF, and SEF) in the context  
513 of a delayed-saccade task (Pierrot-Desilligny et al. 2004). Subjects performed  
514 trials of delayed-saccades that were repeated with the remembered target at  
515 the same location in either retinal or non-retinal coordinates. Within all regions,  
516 significant suppression effects were observed in relation to repetition of the  
517 target location in retinal coordinates (Figures 3-5). We found the time course of  
518 retinal suppression to show the strongest attenuation effects during the delay  
519 period, reflecting the important role of these regions in preparing the saccade.  
520 Slight non-retinal suppression effects were observed during the delay interval  
521 only, but these did not reach statistical significance.

522 We also investigated the lateralization of activity in the hemispheres  
523 when targets were presented ipsi- or contralateral in either retinal (eye-  
524 centered) or non-retinal (head/body/space centered) coordinates. This revealed  
525 a bias to contralateral target locations in the IPS and FEF, defined in reference  
526 to the eye, which is consistent with the retinal repetition suppression effects (Fig  
527 6). We emphasize that the clear laterality found in the IPS and FEF should not  
528 be taken to imply that the areas do not respond to ipsilateral targets, but just that  
529 the response is stronger on the contralateral side. This also explains why we  
530 found retinal suppression effects in both hemispheres (Fig 3).

531 These findings confirm previous fMRI results on the topographic  
532 representation of saccadic movements in IPS and FEF (Sereno et al. 2001;  
533 Schluppeck et al. 2005; Kastner et al. 2007; Hagler and Sereno 2006;  
534 Medendorp et al. 2006; Curtis and D'Esposito 2006; Curtis and Connolly 2008).

535 Medendorp et al. (2003) exploited the topography to demonstrate the updating  
536 of parietal activation when an eye movement changes the remembered location  
537 a visual target across hemifields. The present findings are also fully consistent  
538 with the coding of such a dynamic retinocentric representation, providing a  
539 novel empirical validation of the RS method for studying the motor system.

540 Our data provides no evidence for a contralateral activation bias in the  
541 SEF, in either retinal or non-retinal coordinates (see Fig 6), which is consistent  
542 with recent fMRI findings by Kastner et al. (2007). Nevertheless, just as LIP and  
543 FEF, the human SEF appears to encode saccadic movements in a retinocentric  
544 frame of reference (see Figs 4 and 5). These findings illustrate that, whereas  
545 these three visuomotor areas process eye-centered saccadic information, their  
546 topographic layouts suggest different use of this information. Under the  
547 assumption that the structural organization of the cerebral cortex follows the  
548 principle of maximizing smoothness of neurally encoded features (Graziano and  
549 Aflalo 2007; Durbin and Mitchison 1990), we infer that spatial features constitute  
550 a relevant dimension for IPS and FEF computations and not for the SEF, in line  
551 with a role of the latter region in operational saccade regulation (Stuphorn et al.  
552 2009), guiding eye movements according to arbitrary sets of visual elements  
553 (Olson 2003; Berdyeva and Olson 2009), and stimulus-response associations  
554 (Chen and Wise 1996; see Nachev et al. 2008, for a review).

555 In support of our interpretations, the virtual absence of non-retinal  
556 suppression effects indicates that the observed retinal suppression effects  
557 cannot be due to general motor habituation or fatigue, but mark the identity of  
558 the underlying neural organization. It has been proposed that RS may be the  
559 result of a 'sharpening' of cortical representations (Wiggs and Martin 1998;

560 Desimone 1996; Grill-and Malach 2001; Vidyasagar et al. 2010). A repeating  
561 stimulus can be coded more efficiently by employing fewer active neurons  
562 (Desimone 1996; Friston 2005). From a Bayesian perspective (Ma et al. 2006;  
563 Vaziri et al. 2006), this can be understood in terms of a target location of the last  
564 trial serving as a prior probability distribution for the next trial. When this prior is  
565 integrated with the new sensory evidence, the network may settle to a tighter  
566 distribution in neural space at the second repetition.

567         Notably, we certainly do not want to claim that the practical absence of  
568 non-retinal suppression indicates the absence of non-retinal coding in the brain.  
569 We cannot exclude that the non-retinal repeat trials induced a different form (i.e.  
570 timing) of adaptation, which we did not detect. Alternatively, this absence may  
571 also relate to our paradigmatic constraints, testing saccades to remembered  
572 visual targets. Other effector systems (e.g. reaching) and sensory modalities  
573 may reveal clear non-retinal suppression effects, but this is something to be  
574 pursued in future experiments.

575         Apart from revealing spatial reference frames, the transient dynamics of  
576 RS during the trial is further informative about functional specialization in the  
577 various regions. The stronger suppression effect during the delay period as  
578 compared to the stimulation period and execution phase (Fig 4 and 5) suggests  
579 a more important role in preparing the saccade than in processing the sensory  
580 aspects of the target. Suppression is also much stronger during planning than  
581 during execution of the eye movement. For eye movement execution, eye-  
582 centered representations must be further transformed, as a function of eye  
583 position, by downstream mechanisms into head-centered (non-retinal)  
584 commands for the ocular muscles (Crawford and Guitton 1997). As Figures 3-5

585 show, we did not observe clear non-retinal suppression effects in these regions.  
586 To explain this, it is important to realize that two physically identical eye  
587 movements require also the same patterns of muscle innervations. Thus  
588 saccade execution would simply not allow for any suppression of activity at the  
589 neuromuscular level. But as our data show, resemblance of this notion is found  
590 even at the cortical level, reflecting a network that is involved in both planning  
591 and executing the movement.

592         When comparing our results to monkey neurophysiological findings, we  
593 should keep in mind that BOLD-imaging mostly reflects the pre-synaptic activity  
594 summed over a large number of neurons (Logothetis 2008; Bartels et al. 2008),  
595 whereas single unit recording reports about the output stage of those  
596 computations. Despite these reservations, the present findings are for the most  
597 part quite consistent with previous neurophysiological experiments in monkeys  
598 (Koyama et al. 2004). Among these are studies which report evidence for an  
599 retinocentric topographic organization of saccade targets in the lateral  
600 intraparietal sulcus (Blatt et al. 1990; Colby 1998; Ben Hamed et al. 2001) and  
601 the FEF (Bruce and Goldberg 1985; Robinson and Fuchs 1969; Schall 1991).  
602 Although many earlier human studies have reported topographic maps in the  
603 IPS and FEF (see above), the underlying reference frame has been much less  
604 studied. The present study, examining the spatial organization across different  
605 eye positions, provides solid evidence for a retinocentric topographic  
606 organization of both regions.

607         Debate exists about a topographic organization of saccade goals in  
608 monkey SEF (Schlag and Schlag-Rey 1987, Tehovnik and Lee 1993; Russo  
609 and Bruce 2000). Various single-unit studies have provided evidence that SEF

610 neurons can encode target locations in a continuum from eye-, to head-, to  
611 body- and object-centered reference frames (Martinez-Trujillo et al. 2004; Olson  
612 2003; Schlag and Schlag-Rey 1987), perhaps to represent all possible  
613 contingencies for different task-related motor functions (Martinez-Trujillo et al.  
614 2004). In contrast, our study has revealed a strong bias towards retinal coding  
615 in the human SEF, and the lack of contralateral activation bias indicated a clear  
616 absence of topographic structure. In addition to the methodological differences  
617 stated above (single-units vs fMRI, see Logothetis 2008), another possible  
618 explanation for the apparent discrepancy is that the head-fixed saccade  
619 conditions here have constrained us probing representations other than those  
620 referenced to the eyes (see also the argument above).

621 In conclusion, the present study exploited fMRI-RS to unveil the frames  
622 of reference employed by frontal and parietal areas during saccade planning.  
623 While our findings advance the understanding of how the human brain  
624 processes spatial information for saccades, they also support the feasibility and  
625 validity of using RS methodology in the sensorimotor domain.

626

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815

816 **Figure legends**

817

818 Figure 1.

819 *A. Experimental paradigm. Upper panel.* A typical novel trial  $t$  started with the  
820 illumination of a fixation LED (F). After 3 s, a saccadic target LED (S) was  
821 flashed for 200 ms in the visual periphery, while subjects kept fixation at F. After  
822 a memory delay period of 3.8 s, F was extinguished, which cued the subject to  
823 make a saccade to S. 1 s later the next trial started. *Lower panels.* In a  
824 subsequent repetition trial  $t+1$ , S could be presented at either the same retinal  
825 location as in the previous trial, while the location was novel in non-retinal  
826 (head-centered) coordinates (left), or at a novel retinal position, but at the same  
827 non-retinal location (right). Alternatively, the targets location could be either  
828 novel or repeated in both coordinate frames (not shown). Both fixation and  
829 target stimulus LEDs were yellow-colored and had the same luminance  
830 (difference in LED luminance in the figure is for clarification purposes only). *B.*  
831 Eye traces of one subject over the time course of 20 trials with F at  $0^\circ$  and S  
832 either at  $-9^\circ$  (black traces) or  $9^\circ$  (gray traces). The subject keeps fixation  
833 throughout the trial, also during target stimulus presentation. After the go cue,  
834 response saccades are consistently made toward the location of the  
835 remembered target.

836

837

838 Figure 2.

839 Brain activation during the oculomotor network localizer trials, averaged across  
840 all 18 subjects ( $P < 0.01$ , FDR-corrected;  $25 \text{ mm}^2$  cluster threshold). Data are

841 presented in 2 anatomical views in neurological convention (*A, B*), and on an  
842 inflated representation of the left hemisphere of one of the subjects (*C, D*). A  
843 parietofrontal network is activated, including areas on the banks of the  
844 intraparietal sulcus (IPS), the frontal eye field (FEF), supplementary eye fields  
845 (SEF) and the left ventral premotor area (PMv).

846

847 Figure 3.

848 Group results. *A,B*. Reconstruction of the hemodynamic responses (in pseudo  
849 z-values, referred to as arbitrary units (a.u.)) in the IPS averaged across all  
850 subjects, for novel (black traces) and repeated trials (gray traces) in retinal (*A*)  
851 and non-retinal (*B*) coordinates. *C, D*. Average difference between repeated  
852 and novel trials, together with 95% confidence intervals. LH, left hemisphere;  
853 RH, right hemisphere. Gray areas indicate the periods over which the  
854 differences between the novel and repeated trials were taken. S, Stimulus; D,  
855 Delay; E, Execution phase.

856

857 Figure 4.

858 Repetition suppression effects in the IPS, FEF, and SEF, at various trial phases  
859 in relation to a retinal (black bars) and non-retinal (white bars) reference frame.  
860 Data (in a.u.) combined across hemispheres. Error bars: SE. \*  $P < 0.05$ ; \*\*  
861  $P < 0.01$ , \*\*\*  $P < 0.001$ .

862

863 Figure 5.

864 Indexing the spatial reference frames across the population of subjects, in the  
865 IPS, FEF, and SEF during the same epochs as in Figure 4. Reference Frame

866 Index (RFI) was computed as the difference between the amount of retinal and  
867 non-retinal RS, normalized by the total amount of RS. Positive values indicate a  
868 dominance of retinal coding, negative values point to non-retinal coding. In all  
869 cases, average RFI across the population is larger than zero ( $p < 0.01$ ).

870

871 Figure 6.

872 Lateralized activity in IPS, FEF and SEF during the delay period, averaged  
873 across subjects. *A.* Difference in BOLD signal (in a.u.), across hemispheres,  
874 between contralateral and ipsilateral target locations in retinal coordinates. A  
875 contralateral bias exists in the IPS and FEF ( $P < 0.001$ ), but not in the SEF  
876 ( $P = 0.78$ ). *B.* Lateralized activity when target locations are expressed in terms of  
877 their non-retinal location. No directional preference for non-retinal targets is  
878 observed in any of the regions. Error bars: SE.

879

880

881 **Tables**

882

883 Table 1. Percentage correct responses ( $\% \pm \text{SD}$ ) and mean reaction times (RT

884  $\pm \text{SD}$ , ms) for each of the four conditions.

Target Location Condition	Performance (%)	RT (ms)
Novel retinal, novel non-retinal	$94.5 \pm 5.3$	$215 \pm 69$
Repeated retinal, novel non-retinal	$93.8 \pm 7.3$	$220 \pm 74$
Novel retinal, repeated non-retinal	$94.7 \pm 6.2$	$215 \pm 83$
Repeated retinal, repeated non-retinal	$96.3 \pm 3.5$	$220 \pm 64$

885

886

887 Table 2. Brain regions activated during saccade planning and execution.

888 Coordinates in mm: x (lateral/medial), y (anterior/posterior) and z

889 (superior/inferior), according to Talairach and Tournoux (Talairach and

890 Tournoux 1988). The t-values represent each area's peak voxel statistic across

891 all subjects.

Anatomical Region	Functional Label	Side	x	y	z	t-Value
Intraparietal sulcus	IPS	L	-18	-59	49	9.60
		R	14	-61	52	7.10
Superior frontal sulcus	FEF	L	-25	-10	53	8.45
		R	21	-6	53	5.81
Medial frontal cortex	SEF	L	-1	-4	57	11.25
		R	2	-4	57	11.26
Precentral sulcus	PMv	L	-55	-2	38	5.73

892

893

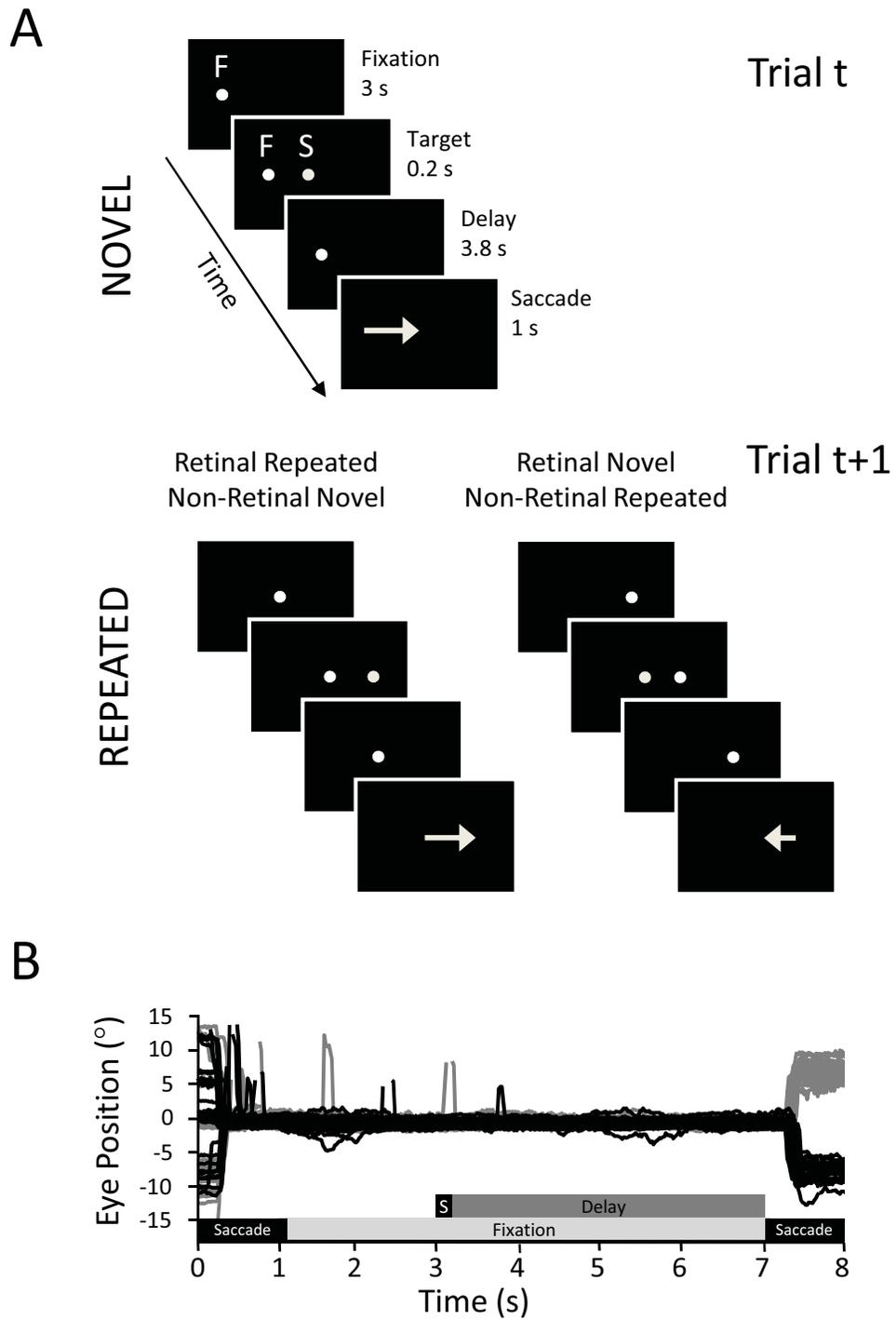


FIGURE 1

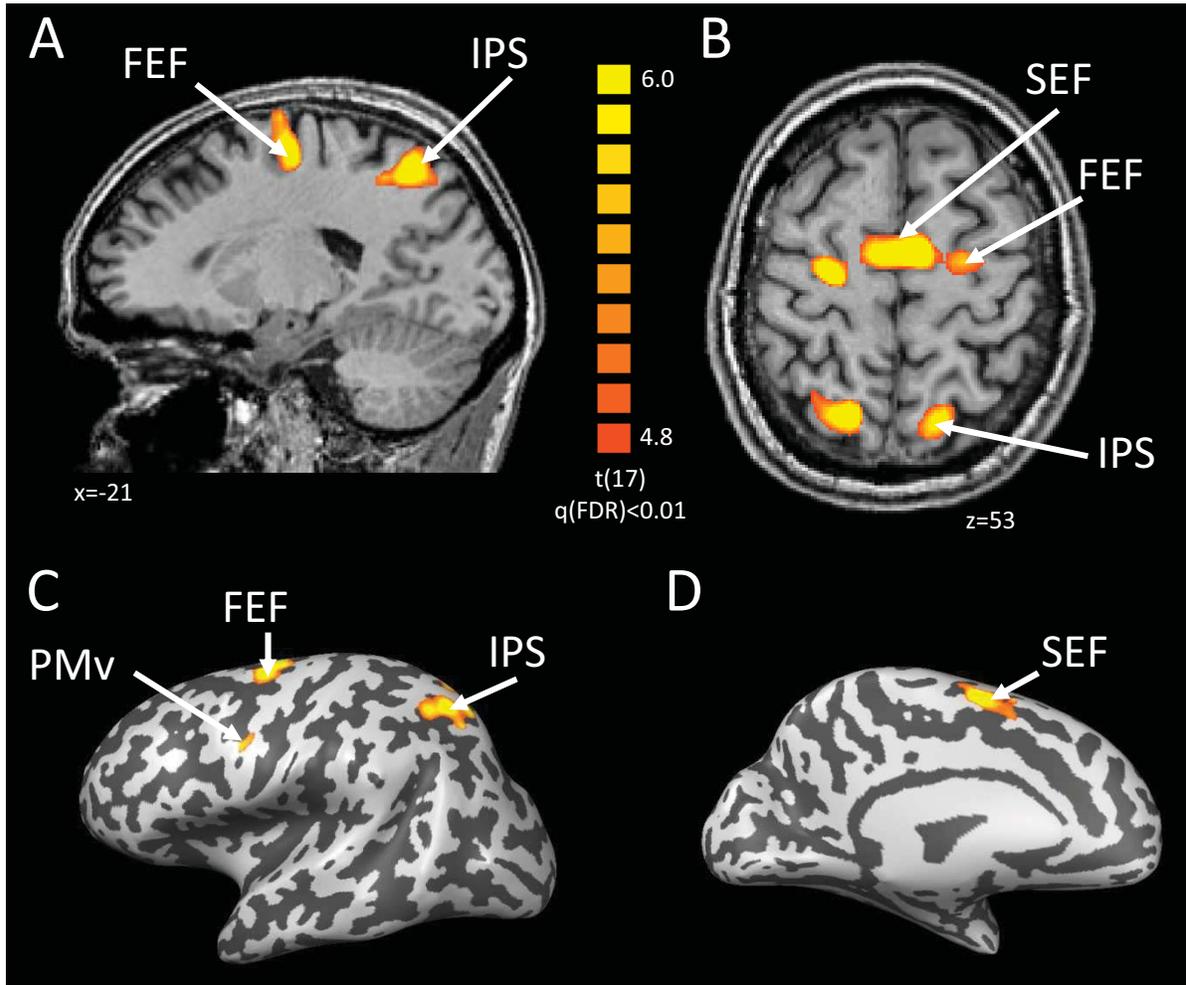


FIGURE 2

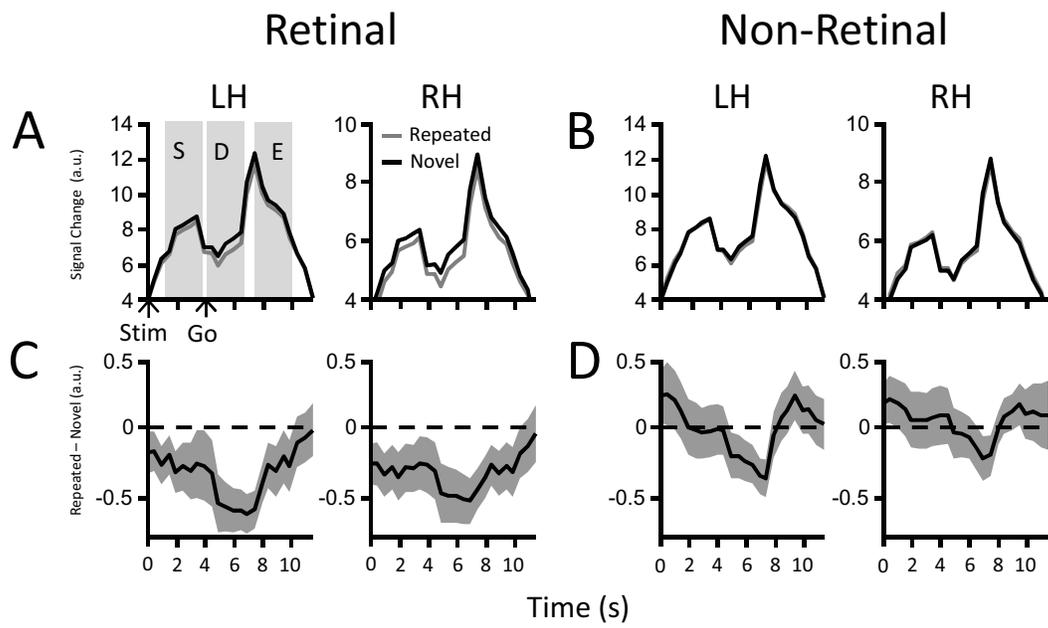


FIGURE 3

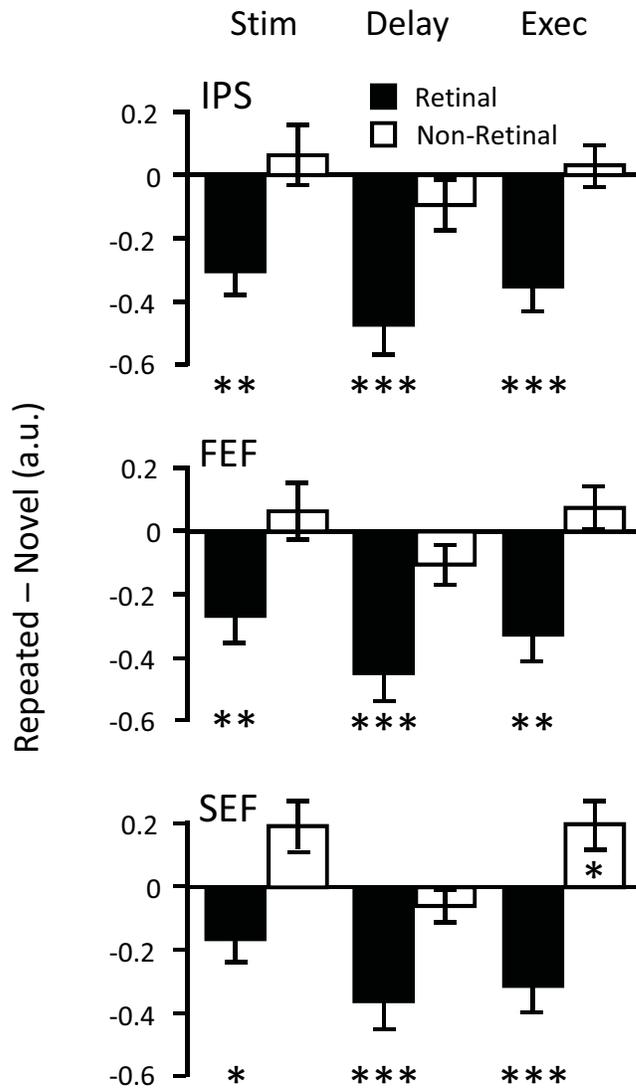


FIGURE 4

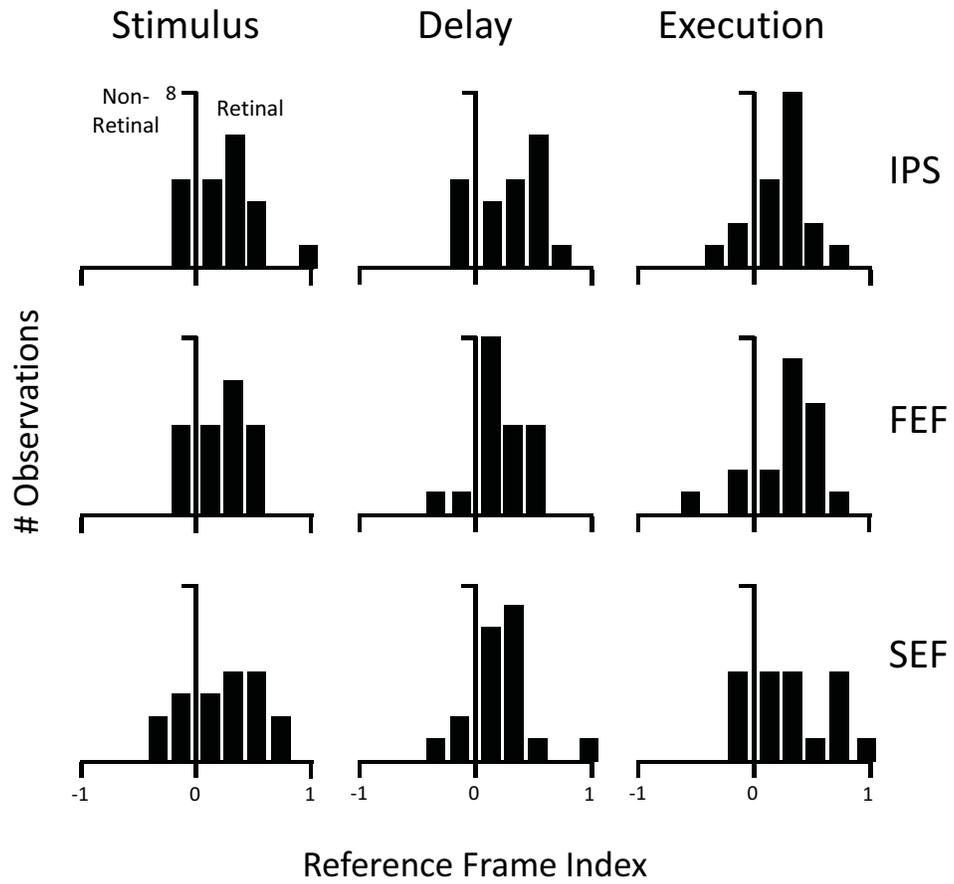


FIGURE 5

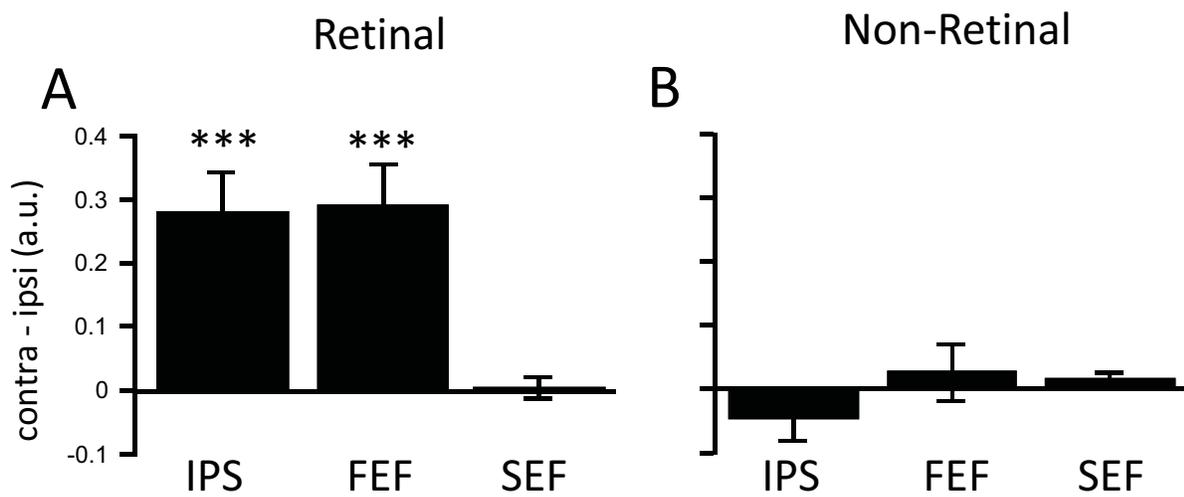


FIGURE 6